ELECTROMYOSTIMULATION—A SYSTEMATIC REVIEW OF THE INFLUENCE OF TRAINING REGIMENS AND STIMULATION PARAMETERS ON EFFECTIVENESS IN ELECTROMYOSTIMULATION TRAINING OF SELECTED STRENGTH PARAMETERS

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ABSTRACT

Filipovic, A, Kleinöder, H, Dörmann, U, and Mester, J. Electromyostimulation-A systematic review of the influence of training regimens and stimulation parameters on effectiveness in electromyostimulation training of selected strength parameters. J Strength Cond Res 25(11): 3218-3238, 2011-Our first review from our 2-part series investigated the effects of percutaneous electromyostimulation (EMS) on maximal strength, speed strength, jumping and sprinting ability, and power, revealing the effectiveness of different EMS methods for the enhancement of strength parameters. On the basis of these results, this second study systematically reviews training regimens and stimulation parameters to determine their influence on the effectiveness of strength training with EMS. Out of about 200 studies, 89 trials were selected according to predefined criteria: subject age (<35 years), subject health (unimpaired), EMS type (percutaneus stimulation), and study duration (>7 days). To evaluate these trials, we first defined appropriate categories according to the type of EMS (local or whole-body) and type of muscle contraction (isometric, dynamic, isokinetic). Unlike former reviews, this study differentiates between 3 categories of subjects based on their level of fitness (untrained subjects, trained subjects, and elite athletes) and on the types of EMS methods used (local, whole-body, combination). Special focus was on trained and elite athletes. Untrained subjects were investigated for comparison purposes. The primary purpose of this study was to point out the preconditions for producing a stimulus above the training threshold with EMS that activates strength adaptations to give guidelines for implementing EMS effectively in strength training especially in high-performance sports. As

a result, the analysis reveals a significant relationship (p < 0.05) between a stimulation intensity of \geq 50% maximum voluntary contraction (MVC; 63.2 \pm 19.8%) and significant strength gains. To generate this level of MVC, it was possible to identify guidelines for effectively combining training regimens (4.4 \pm 1.5 weeks, 3.2 \pm 0.9 sessions per week, 17.7 \pm 10.9 minutes per session, 6.0 \pm 2.4 seconds per contraction with 20.3 \pm 9.0% duty cycle) with relevant stimulation parameters (impulse width 306.9 \pm 105.1 microseconds, impulse frequency 76.4 \pm 20.9 Hz, impulse intensity 63.7 \pm 15.9 mA) to optimize training for systematically developing strength abilities (maximal strength, speed strength, jumping and sprinting ability, power).

KEY WORDS strength training, electromyostimulation, review, training parameters, EMS methods, trained athletes

INTRODUCTION

egarding the influence of electromyostimulation (EMS) methods on strength abilities, our first study revealed the effectiveness of different EMS methods for enhancing maximal strength, speed strength, jumping and sprinting ability, and power (35). Significant gains (p < 0.05) were shown in maximal strength (isometric Fmax +32.6 ± 17.6%; dynamic Fmax +31.6 ± 18.8%), speed strength (eccentric isokinetic Mmax +27.7 ± 8.5%; concentric isokinetic Mmax +20.5 ± 11.5%; rate of force development (RFD) +44.8 ± 27.8%; force impulse $+19.2 \pm 5.8\%$; zmax $+19 \pm 0\%$; and power $+47.8 \pm 14.9\%$). Developing these parameters increases vertical jump height by +15.5 ± 4.9% (squat jump [SJ] 12.9 ± 7.0%, countermovement jump [CMJ] +14.5 ± 5.8%, drop jump [DJ] +9.3 ± 3.8%) and improves sprint times by as much as −2.8 ± 1.7% in trained and elite athletes.

Compared to traditional voluntary strength training, several EMS parameters have to be considered in addition to common training regimen for training control of strength training with EMS. This complexity of different combinations

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of training regimen and stimulation parameters makes it difficult to systematically implement EMS.

In voluntary strength training, the resistance of additional weight regulates the training intensity because of the maximum voluntary contraction (MVC), which is defined as 1 repetition maximum. In contrary to voluntary exercise EMS activates muscle contraction artificially without using a resistance load. For this reason, it is not possible to simply transfer conventional training regimens into strength training with EMS. Despite the difference in muscle activation, the design of most EMS studies leaned heavily on traditional strength training parameters (cf. (5,22,34,55,75,76)). Several studies showed that electrical stimulus can be more intense than voluntary stimulus activated by the central nervous system (cf. (12,13,37,41,72)). They showed that EMS can cause significantly higher creatinkinase activity and thus might cause more damage in the individual's muscular system, which in turn would lengthen the regeneration time required between sessions.

In contrast to voluntary strength training, the MVC in EMS strength training is regulated according to the level of stimulation parameters. In turn, these parameters depend on the individual condition of the muscular system and on individual pain perception. In most EMS studies, 100% MVC was defined under voluntary maximal isometric conditions in an entry test. The level of stimulation intensity within the stimulation period was defined under EMS conditions and documented as a percentage of the MVC for the entry test performed under voluntary conditions. With regard to the MVC level, EMS research shows values of >100% with EMS. Under voluntary conditions, it is difficult to reach the absolute maximum level of contraction because accomplishing this depends on the individual's level of strength and motivation. Some studies revealed that elite athletes with a high level of maximal strength are able to reach levels of MVC close to the absolute maximum (100%). Average subjects only reach their maximum in extreme situations. For this reason, EMS could enable strength training at intensities that are otherwise difficult to reach because of the personal motivation levels. However, also in EMS training, the level of stimulation intensity (MVC) depends on individual pain perception with regard to the stimulation parameters and thus also indirectly depends on motivation.

In this review series, the selected studies, although collectively concerning the improvement of strength abilities, differed in stimulation patterns and training designs. More precisely, the studies vary in the type of EMS methods, training regimen, stimulation parameters, subject age and physical condition, group sizes, type of control groups, test designs, and parameters and in the EMS equipment used (EMS device and electrodes). All of these varying parameters in combination may influence the study outcome to a different degree and thus complicate the comparison of the results.

This second review out of our 2-part series reports data exclusively in relation to the results of the first study, which investigated the effects of EMS on selected strength parameters (cf. (30)). Therefore, the objectives of this second article are to examine the influence of the relevant training regimen and stimulation parameters on effectiveness; to identify a combination of training regimen and stimulation parameters for producing a stimulus that activates strength adaptations of the individuals' muscular system; to make recommendations for training control to enhance maximal strength, speed strength, and motor abilities such as jumping and sprinting.

METHODS

Search for and Selection of Eligible Studies

For the investigative process, we first concentrated on studies focussing on strength gains in skeletal muscles of healthy subjects with nonclinical background to filter the amount of EMS studies. As a result, about 200 studies were collected that were performed between 1965 and 2008. About 60% of them were found with the help of scientific search engines such as Medline and Pubmed and directly on journal data bases such as JSCR (Keywords: electrical stimulation, EMS, strength training, trained athletes, elite athletes). The other 40% were found through references within these studies.

To maximize the number of comparable trials (randomized controlled trails [RCTs]), certain preconditions were set: (a) Subjects: healthy, unimpaired subjects with ≤35 years of age; (b) Type of stimulation: percutaneaus EMS with the aim of enhancing strength abilities of both the upper and lower body; and (c) Study design: minimum study duration of ≥7 days, comparable tests such as pretests, posttests, and retests.

Only studies with homogeneous groups on a comparable level of fitness were considered in this review. Significant gains for the training group were documented in relation to the baseline and the difference to the control group in posttesting (cf. (30)).

Data Classification

The review began by selecting a total of 59 studies. From this pool of investigations, all trials in which male and female subjects formed different training groups or in which >1 EMS group (with different EMS methods) was trained or tested with different parameters were once again divided into individual trails (cf., e.g., (21,60)). For example, studies investigated 2 types of EMS methods, the trials were split and each was sorted to a specific subgroup (e.g., isometric EMS, combination EMS).

All in all, 89 trials were emphasized from the original 59 studies. These trials were analyzed, compared, and presented in a comprehensive table.

To represent this large number of studies and their results clearly, the trials were classified according to the type of EMS method (local EMS methods—stimulation of defined muscle groups with single electrodes; whole-body EMS methods stimulation and activation of several muscle groups simultaneously through an electrode belt system, agonist and

antagonist are activated at the same time) and type of muscle contraction (e.g., isometric EMS, dynamic EMS [includes isokinetic]). The combination EMS method is a subgroup for both types of stimulation. In combination methods, the types described above are combined with additional specific training (e.g., conventional weight training, plyometric jump training).

Besides these categories, the review primarily differentiated between the subjects' individual levels of fitness: untrained subjects (no experience in strength training, no regular exercise before study); trained subjects (experience in strength training, regularly exercising up to 3 sessions per week); elite athletes (systematically training on a high-performance level >3 sessions per week).

Data Extraction

The data from the analyzed studies were sorted and presented in tables. To enable accurate categorization and to provide a layout for evaluating and comparing several different studies at the same time, all of the tables were based on the same parameters (cf. Tables 1 and 2).

Statistical Analyses

To analyze the data, different groups and subgroups were formed (cf. data classification). For evaluation, we assigned mean and SD of the data (training regimen and stimulation parameters) of meaningful studies in each category and subgroup. To compare the results and point out relationships between certain parameters, extreme data were eliminated.

Special focus was on trained and elite athletes. Untrained subjects were investigated for comparison purposes.

In references to significance levels or confidence intervals, an α -level of 0.05 was used, which corresponds to 95% confidence intervals. For correlation comparisons, the level of significance was established at $p \leq 0.05$.

RESULTS OF THE SEARCH AND SELECTION PROCESS

The analysis of the selected studies showed that more than half of the trials tested male subjects. Studies involving female subjects only or a mixed sample had a stake of 20%. Only 7 studies did not differentiate with details on gender.

On average, the subjects were 22.8 years old at the time of the pretest for the trials. All subjects were classified as healthy and unimpaired and had no history of injury in the tested muscle group. The trials covered a period between 10 days and 14 weeks. On average, 10.6 ± 5.1 subjects were examined over an average of 5 ± 2.3 weeks (cf. Table 3). However, the majority of the studies (68%) contained a stimulation period of 4–6 weeks. The number of training sessions varied from 1 to 7 sessions per week. An average of 16.3 ± 6.8 sessions was completed within the training period, with a duration of 17.6 ± 10.7 minutes per session (cf. Tables 4–6).

Regarding the locality of the stimulated muscles, the analysis showed that the lower body was the main object of the trials (75%). Furthermore, the study showed that the m. quadriceps femoris (60%) was the most examined muscle. In contrast, only

Fully extension = 180° Stimulation combination dynamic sometric, whole-Training regimen Session ai: of contractions Contractions session per session biceps brachi; RA = rectus abdominis; TB = triceps brachi Number Sessions ser week Ses/wk Study period (wks) regimen and training of sessions Sessions Number **TABLE 1.** Data extraction of subject information Untrained of fitness QF = quadriceps femoris; BB Ø Years Age Gender mean; ı Ø

| | | | | Stimulat | tion paramet | ters | | | | |
|---|---------------------------------------|---|------------------|----------------------|-------------------|-------------------------|--|--|--------------------------|---|
| Type of current | Type of stimulator | Impulse form | Impulse width | Impulse frequency | Impulse intensity | Impulse on-time | Impulse interval | Duty-cycle | Rise/fall | Stimulation intensity |
| Biphasic Monophasic Alternating Russian Interference current | Type or brand of EMS stimulator | Sinus, rectangular, triangular, 2-peak, etc. | (μs) | (Hz) | (mA) | Contraction time on (s) | Time between 2 single impulses off (s) | Stimulation ratio, relation between on and off-time | Impulse, ramp time | Percentage maximum voluntary contraction |

| Table 3. Overview of mean values for the training regimen and stimulation parameters. | TABLE 3. Overview | of mean values | for the training | regimen and | stimulation | parameters.* |
|---|-------------------|----------------|------------------|-------------|-------------|--------------|
|---|-------------------|----------------|------------------|-------------|-------------|--------------|

| | | Ti | raining regime | en | | | | Impulse | On-time | Interval | Intensity |
|-----------|---------------|---------------|----------------|--------------|----------------|------------------|----------------|----------------|---------------|----------------|----------------|
| 89 Trials | Subjects | Age | Sessions | Weeks | Min | Width (μs) | Frequency (Hz) | intensity (mA) | On (s) | Off (s) | %MVC |
| Mean (SD) | 10.6 (5.0) | 22.9 (2.8) | 16.5 (6.8) | 5.1 (2.3) | 17.7 (10.9) | 266.3 (133.0) | 68.8 (31.8) | 59.6 (32.3) | 10.2 (8.0) | 42.4 (48.7) | 59.5 (25.3) |

^{*%}MVC = percentage maximum voluntary contraction.

TABLE 4. Overview training regimen 1/3. Subjects. Training regimen Level of Sessions Contractions/ t Authors n Sex fitness Sessions Weeks per wk sessions (min) EMS method Muscle Stim Age QF 10 W 20.9 3S/10Rep/3Int Avila, et al. (5) Trained Dynamic Avila, et al. (5) 10 M 21 Trained 8 2.0 3S/10Rep/3Int Dynamic QF 4 Speicher and 10 M/W 23.19 Trained 2.0 30 Iso/combination/ WB-EMS 8 4 150-100 Kleinöder (69) (sport student) dvn WB QF Paillard I (60) 9 M 25.5 Trained (student) 15 5 3.0 15 Isometric 90 QF Paillard II (60) 10 M 25.5 Trained (student) 3.0 90 15 5 60 Isometric Babault et al. (6) Elite (rugby) 36 QF/TS/GM 60/90/ 15 M 22 24 12 2.0 12 Isometric Trained (student) Holcomb (33) 8 M/W 23.5 12 15 BB 90 4 3.0 15 Isometric 100 Rep(conc)/ Matsuse (52) 6 M 23.6 Untrained 24 8 3.0 16 Isometric BB/TB 60 100 rep(ecc) TS Jubeau et al. (38) 10 M 24 16 4 4.0 18 90 Untrained Isometric Gondin et al. (31) 9 M 24.7 Untrained 32 8 4.0 40 18 Isometric QF 120 Maffiuletti et al. (49) 29 18 40 QF 90 1 M Untrained 4.5 20 Isometric Boeckh-Behrens 22 M Trained (sport student) 12 2.0 Iso WB WB-EMS 6 5 and Mainka (13) 22 M 12 2.0 Boeckh-Behrens Trained (sport student) 6 Iso WB WB-EMS 10 and Mainka II (13) Kreuzer (41) 9 M 16.78 Trained (water polo) 8 2.0 Iso/combination WB-EMS 4 WB QF Gondin et al. (31) 12 M 23.5 Untrained 32 8 4.0 40 18 Isometric 120 QF Brocherie et al. (19) 9 M 22.6 Elite (ice hockey) 9 3 3.0 30 19 Isometric 120 Boeckh-Behrens I (12) 21 M 22.3 Trained (sport student) 12 6 2.0 15 Iso WB WB-EMS Boeckh-Behrens II (12) 20 M 22.3 Trained (sport student) 12 6 2.0 15 Iso WB WB-EMS Isometric Herrero et al. (32) 19 Untrained 8 2.0 53 OF 120 11 M 34 Herrero et al. (32) Untrained 16 QF 120 10 M 19 4.0 53 34 Isocombination OF Parker et al. (61) 7 M/W 23.2 Untrained 8 2.0 10 10 Isometric 120 Parker et al. (61) 20 M/W 23.2 Untrained 12 3.0 10 Isometric QF 120 10 Malatesta et al. (50) Elite (volleyball) 12 3.0 20-22 QF/TS 90/90 12 M 17.2 12 Isometric Trained (sport student) Boeckh-Behrens (14) 26 M 21.7 12 6 2.0 45 Iso/combination WB-FMS WB QF Dervisevic et al. (26) 20 M 24.2 Trained (sport student) 30 10 3.0 15 Iso/combination 120 Bircan et al. (10) 10 M/W 23.2 Untrained 15 3 5.0 15 Isometric QF 180 Bircan et al. (10) 10 M/W 23.2 QF 180 Untrained 15 3 5.0 15 Isometric Bircan et al. (10) 10 M/W 23.2 Untrained 15 3 5.0 OF 180 15 Isometric WB = whole-body.

| | THE | Su | bjects // | | | | Training regimen | | | | |
|------------------------------------|-------|------|--------------------------|----------|-------|------------|------------------------------|---------|------------------|--------|----------------|
| Authors | n Sex | Age | Level of fitness | Sessions | wks S | Ses per wk | Contractions/sessions | t (min) | EMS method | Muscle | Stim |
| Maffiuletti et al. (47) | 10 M | | Elite (volleyball) | 12 | 4 | 3.0 | 48/30 + 50Plyo | 26 | Combination | QF/TS | 110/10 |
| Maffiuletti et al. (47) | 10 M | 21.8 | Elite (volleyball) | 12 | 4 | 3.0 | 48/30 | 26 | Isometric | QF/TS | 110/10 |
| Maffiuletti et al. (48) | 8 M | 20.4 | Untrained | 16 | 4 | 4.0 | 45 | 18 | Isometric | TS/TA | 90 |
| Boeckhh-Behrens and Treu (15) | 20 M | 22.4 | Trained (sports student) | 12 | 6 | 2.0 | 5 | 25 | Iso WB | WB-EMS | |
| Maffiuletti et al. | 10 M | 24.7 | Elite (basketball) | 12 | 4 | 3.0 | 48 | 16 | Isometric | QF | 120 |
| Colson et al. (22) | 9 M | 24 | Trained (student) | 21 | 7 | 3.0 | 5S/6Rep/3Int | | Isometric | BB | 90 |
| Hortobagyi et al. (35) | 8-W | 24.8 | Untrained | 24 | 6 | 4.0 | 35 | | Dyn (isokinetic) | QF | 90 dyn |
| Willougby and Simpson (76) | 5 W | 20 | Trained athletes | 18 | 6 | 3.0 | | | Isometric | QF | , |
| Willougby and Simpson (76) | 5 W | 20 | Trained athletes | 18 | 6 | 3.0 | 3S/8-10Rep /3Int (85%1RM) | | Dyn/isokinetic | QF | dyn |
| Hortogagyi et al. (34) | 8 W | 26.3 | Untrained | 24 | 6 | 4.0 | 4-6S/6-8Rep/1Int | | Dyn (isokinetic) | QF | 120 |
| Willoughby and Simpson (75) | 6 M | | Elite (basketball) | 18 | 6 | 3.0 | 10 | 10 | Isometric | BB | 180 |
| Willoughby and Simpson (75) | 6 M | 20 | Elite (basketball) | 18 | 6 | 3.0 | 3S/8-10Rep/3Int | 10 | Dyn/isokinetic | BB | 180°-30 |
| Pichon et al. (62) | 7 | 23 | Elite (swimming) | 9 | 3 | 3.0 | 27 | 12 | Isometric | LD | 140° arms |
| Martin et al. (51) | 6 M | | Untrained | 12 | 4 | 3.0 | | 10 | Isometric | TS | Full dorsi fle |
| Miller and Thepaut-Mathieu (55) | 16 M | 23.3 | Trained (student) | 15 | 5 | 3.0 | 5S/5Rep/3Int | | Isometric | BB | 155 |
| Balogun et al. (8) | 10 M | 22 | Untrained | 18 | 6 | 3.0 | Max | | Isometric | QF | 120 |
| Balogun et al. (8) | 10 M | 22 | Untrained | 18 | 6 | 3.0 | Max | | Isometric | QF | 120 |
| Balogun et al. (8) | 10 M | | Untrained | 18 | 6 | 3.0 | Max | | Isometric | QF | 120 |
| Rich (64) | 12 W | 21 | Ontramod | 18 | 6 | 3.0 | Hillian | | Isometric | TB | 90 |
| Rich (64) | 12 M | 21 | | 18 | 6 | 3.0 | | | Isometric | TB | 90 |
| Rich (64) | 12 W | 21 | | 18 | 6 | 3.0 | | | Isometric | BB | 90 |
| Rich (64) | 12 M | 21 | | 18 | 6 | 3.0 | | | Isometric | BB | 90 |
| Portmann and Montpetit (63) | | 24 | Trained athletes | 24 | 8 | 3.0 | 10 | | Dyn/isokinetic | QF | 90-180 |
| Portmann and Montpetit (63) | | 24 | Trained athletes | 24 | 8 | 3.0 | 10 | | Iso/combination | | 90 |
| Venable et al. (73) | 13 M | 19 | Untrained | 15 | 5 | 3.0 | 10 | 12 | Iso/combination | | 145/130/1 |
| Delitto et al. (25) | 1 M | 27 | Elite (weightlifter) | | 16 | 1.1 | 10 | 30 | Isometric | QF | 115 |
| Soo et al. (68) | 6 W | 25.2 | | 10 | 5 | 2.0 | 8 | | Isometric | QF | 120 |
| Soo et al. (68) | 9 M | 25.2 | | 10 | 5 | 2.0 | 8 | | Isometric | ΩF | 120 |
| Lai et al. (43) | | | Untrained | 15 | 3 | 5.0 | 3S/10Rep/1Int | | Isometric | QF | 120 |
| Lai et al. (43) | | | Untrained | 15 | 3 | 5.0 | 3S/10Rep/1Int | | Isometric | QF | 120 |
| Cabric and Appell (21) | 6 W | | Trained (sports student) | 14 | 2 | 7.0 | 10 | | Isometric | TS | 10 |
| Cabric and Appell (20) | 12 M | 21.5 | Trained | 21 | 3 | 7.0 | 15-25 | | Isometric | TS | 10 |

^{*1}RM=1 repetition maximum; Dyn=dynamic; TS=triceps surae; QF=quadriceps femoris; RA=rectus abdominis; BB=biceps brachii; LD=latissimus dorsi; TB=triceps brachii; TA=tibialis anterior; UB=upper body; GM=gluteus muscles; WB=whole body.

| Cabric and Appell (20) 12 M 21.5 Trained 21 3 7.0 15–25 Isometric TS 10 Kubiak et al. (42) 10 M/W 24 Untrained 15 5 3.0 19 Isometric QF 120 Alon et al. (1) 8 M/W 30 Untrained 12 4 3.0 Isometric RA 0 Alon et al. (1) 8 M/W 30 Untrained 12 4 3.0 Isometric RA 45 St. Pierre et al. (70) 3 W 20 Trained 7 1.5 4.7 10 Isometric QF 90 WeeksIf et al. 9 M 32.2 Elite (tennis) 24 6 4.0 5 Set of max V diff 's WeeksIf et al. 9 M 32.2 Elite (tennis) 24 6 4.0 5 Set of max V diff 's WeeksIf et al. (57) 9 W 20.89 Trained (student) 18 6 3.0 10 Dyn (isokinetic) QF 90 Selkowtz (67) 9 W 21.22 Trained (student) 18 6 3.0 3S/6Rep Dyn (isokinetic) QF 90 Stefanovska Vodovnik (71) 5 Stefanovska Vodovnik (71) 5 V22.5 Untrained 24 4 6.0 10 Isometric QF 120 Mohr et al. (56) 6 W 25 Untrained 15 3 5.0 10 Isometric QF 120 Mohr et al. (29) 19 M 27.5 Untrained 18 6 3.0 10 Isometric QF 120 Currier and Mann (24) 8 M/W 24 Untrained 15 5 3.0 10 Isometric QF 120 Currier and Mann (24) 9 M/W 24.0 Untrained 18 6 3.0 10 Isometric QF 120 Currier and Mann (24) 9 M/W 24.0 Untrained 15 5 3.0 10 Isometric QF 120 Currier and Mann (24) 9 M/W 24.1 Untrained 15 5 3.0 10 Isometric QF 120 Currier and Mann (24) 9 M/W 24.1 Untrained 15 5 5.0 10 Isometric QF 120 Owens and Malone (59) 10 M/W 21.3 Intrained 25 5 5.0 10 Isometric QF 120 Covens and Malone (59) 10 M/W 21.3 Intrained 10 1.5 6.7 10 Isometric QF 120 Covens and Malone (59) 10 M/W 21.3 Intrained 10 1.5 6.7 10 Isometric QF 145 McMiken et al. (86) 9 W 21.8 Untrained 15 5 5.0 ca. 24 12 Isometric QF 145 McMiken et al. (88) 4 22 Trained (student) 15 4 3.8 6 6 6 Isometric QF 145 McMiken et al. (88) 4 22 Trained (marines) 9 Untrained S2 8 6.5 Isometric QF 10 Isometric QF 145 McMiken et al. (88) 4 22 Trained (marines) 9 Untrained S2 8 6.5 Isometric QF 10 Isometric QF 145 McMiken et al. (89) 19 M/W 21.3 Intrained (student) 15 4 3.8 6 6 6 Isometric QF 10 Massey et al. (80) 10 Isometric QF 10 Mit S0 Isometric QF 10 Massey et al. (80) 10 Isometric QF 10 Isometric | | | 240 | Subject | s | 2 | | | Training reg | imen | | | |
|--|------------------------|-----------|-----|-----------|-------------------|----------|-------|----------|--------------|-----------|-----------------|--------|---------------------|
| Kubiak et al. (42) 10 M/W 24 Untrained 15 5 3.0 19 Isometric QF 120 | Authors | n | Sex | Age | Level of fitness | Sessions | Weeks | | | | | Muscle | e Stim ^o |
| Alon et al. (1) | Cabric and Appell (20) | | М | 21.5 | | 21 | | | 15-25 | | Isometric | | |
| Alon et al. (1) | Kubiak et al. (42) | 10 | M/W | | Untrained | 15 | 5 | | 19 | | Isometric | | 120 |
| St. Pierre et al. (70) | Alon et al. (1) | 8 | M/W | 30 | Untrained | 12 | 4 | 3.0 | | | Isometric | RA | 0 |
| St. Pierre et al. (70) 7 M 20 Trained 7 1.5 4.7 10 Isometric QF 90 | Alon et al. (1) | 8 | M/W | 30 | Untrained | 12 | 4 | 3.0 | | | Isometric | RA | 45 |
| Weekslf et al. 9 M 33.2 Elite (tennis) 24 6 4.0 5 Set of max Dyn/isokinetic QF | St. Pierre et al. (70) | 3 | W | 20 | Trained | 7 | 1.5 | 4.7 | 10 | | Isometric | QF | 90 |
| Nobbs et al. (57) 9 W 20.89 Trained (student) 18 6 3.0 10 Dyn (isokinetic) QF 45 Nobbs et al. (57) 9 W 21.22 Trained (student) 18 6 3.0 3S/6Rep Dyn (isokinetic) QF 90–18 Selkowitz (67) 8 M/W 24.6 Trained (student) 12 4 3.0 10 Isometric QF 120 Stefanovska Vodovnik (71) 5 22.5 Untrained 24 4 6.0 10 Isometric QF 120 Mohr et al. (56) 6 W 25 Untrained 15 3 5.0 10 Isometric QF 120 Isometric QF 145 Is | St. Pierre et al. (70) | 7 | M | 20 | Trained | 7 | 1.5 | 4.7 | 10 | | Isometric | QF | 90 |
| Nobbs et al. (57) 9 W 21.22 Trained (student) 18 6 3.0 3S/6Rep Selkowitz (67) 8 M/W 24.6 Trained (student) 12 4 3.0 10 Isometric QF 120 Isometric QF 145 Isometric QF 150 Isometric QF 100 Iso | Weekslf et al. | 9 | M | 33.2 | Elite (tennis) | 24 | 6 | 4.0 | | xV | Dyn/isokinetic | QF | |
| Nobbs et al. (57) 9 W 21.22 Trained (student) 18 6 3.0 3S/6Rep Selkowitz (67) 8 M/W 24.6 Trained (student) 12 4 3.0 10 Isometric QF 120 Isometric QF 145 Isometric QF 150 Isometric QF 100 Iso | Nobbs et al. (57) | 9 | W | 20.89 | Trained (student) | 18 | 6 | 3.0 | 10 | | Dyn (isokinetic | QF | 45 |
| Selkowritz (67) 8 M/W 24.6 Trained (student) 12 4 3.0 10 Isometric QF 120 | Nobbs et al. (57) | 9 | W | 21.22 | Trained (student) | 18 | 6 | | 3S/6Rep | | Dyn (isokinetic | QF | 90-180 |
| Boutelle-et al. (17) 9 M/W 26 22.5 Untrained 24 4 6.0 10 Isometric QF 120 | Selkowitz (67) | 8 | M/W | 24.6 | Trained (student) | 12 | 4 | 3.0 | | | | | 120 |
| Stefanovska Vodovnik (71) 5 22.5 Untrained 24 4 6.0 10 Isometric QF 120 | Boutelle et al. (17) | 9 | M/W | 26 | | 20 | | 5.0 | /10 | | Isometric | QF | 150 |
| Stefanovska Vodovnik (71) 5 22.5 Untrained 24 4 6.0 10 Isometric QF 120 | | 5 |) | 22.5 | Untrained | 24 | 4 | 6.0 | / | 10 | Isometric | QF | 120 |
| Mohr et al. (56) 6 W 25 Untrained 15 3 5.0 10 Isometric QF 120 Fahey et al. (29) 19 M 27.5 Untrained 18 6 3.0 15 Isometric QF 115 Fahey et al. (29) 19 M 27.5 Untrained 18 6 3.0 15 Isometric QF 180 Currier and Mann (24) 8 M/W 24 Untrained 15 5 3.0 10 Isometric QF 120 Currier and Mann (24) 9 M/W 24 Untrained 15 5 3.0 10 Isometric QF 120 Currier and Mann (24) 9 M/W 24 Untrained 15 5 3.0 10 Isometric QF 120 Currier and Mann (24) 9 M/W 23.5 Untrained 15 5 3.0 10 Isometric QF 120 | | 5 | | | | 24 | 4 | | | 10 | Isometric | QF | 120 |
| Fahey et al. (29) 19 M 27.5 Untrained 18 6 3.0 10 Isometric QF 120 Currier and Mann (24) 9 M/W 24 Untrained 15 5 3.0 10 Isometric QF 120 Laughman et al. (45) 20 M/W 23.5 Untrained 25 5 5.0 10 Isometric QF 120 Owens and Malone (59) 10 M/W 21 Untrained 10 1.5 6.7 10 Isometric QF 145 Owens and Melone (59) 10 M/W 21 Untrained 5 1.5 3.3 10 Isometric QF 145 McMiken et al. (54) 9 M/W 21.3 10 3 3.3 10 Isometric QF 150 Romero et al. (65) 9 W 21.6 Untrained 10 5 2.0 15 Isometric QF 150 Eriksson et al. (28) 9 20 Trained (student) 25 5 5.0 ca. 24 12 Isometric QF 90 Kots and Chwilon (39) 16 17 Trained (judo) 16 2.5 6.4 10 10 Isometric TS Kots and Chwilon (39) 19 10 M 18 Untrained 52 8 6.5 Isometric QF 90 Massey et al. (52) 16 M 22 Trained (marines) 9 40 Isometric QF 90 Massey et al. (52) 16 M 22 Trained (marines) 9 40 Isometric QF 90 Massey et al. (52) 16 M 22 Trained (marines) 9 | Mohr et al. (56) | 6 | W | | Untrained | 15 | 3 | 5.0 | 10 | | Isometric | QF | 120 |
| Currier and Mann (24) 8 M/W 24 Untrained 15 5 3.0 10 Isometric QF 120 Currier and Mann (24) 9 M/W 24 Untrained 15 5 3.0 10 Isometric QF 120 Laughman et al. (45) 20 M/W 23.5 Untrained 25 5 5.0 10 12.50 Isometric QF 120 Owens and Malone (59) 10 M/W 21 Untrained 10 1.5 6.7 10 Isometric QF 145 Owens and Melone (59) 10 M/W 21 Untrained 5 1.5 3.3 10 Isometric QF 145 Owens and Melone (59) 9 M/W 21.3 10 3 3.3 10 Isometric QF 145 McMiken et al. (54) 9 M/W 21.3 10 3 3.3 10 Isometric QF 150 | Fahey et al. (29) | 19 | М | 27.5 | Untrained | 18 | 6 | 3.0 | | 15 | Isometric | QF | 115 |
| Currier and Mann (24) 8 M/W 24 Untrained 15 5 3.0 10 Isometric QF 120 Currier and Mann (24) 9 M/W 24 Untrained 15 5 3.0 10 Isometric QF 120 Laughman et al. (45) 20 M/W 23.5 Untrained 25 5 5 5.0 10 12.50 Isometric QF 120 Owens and Malone (59) 10 M/W 21 Untrained 10 1.5 6.7 10 Isometric QF 145 Owens and Melone (59) 10 M/W 21 Untrained 5 1.5 3.3 10 Isometric QF 145 McMiken et al. (54) 9 M/W 21.3 10 3 3.3 10 Isometric QF 150 Romero et al. (65) 9 W 21.6 Untrained 10 5 2.0 15 Isometric QF 115 Eriksson et al. (28) 9 20 Trained (student) 25 5 5.0 ca. 24 12 Isometric QF 90 Eriksson et al. (28) 4 22 Trained (student) 15 4 3.8 6 6 Isometric QF 90 Kots and Chwilon (39) 16 17 Trained (judo) 16 2.5 6.4 10 10 Isometric TS Kots and Chwilon (39) 19 10 M 18 Untrained 52 8 6.5 Isometric QF 90 Massey et al. (52) 16 M 22 Trained (marines) 9 40 Isometric UB Diff. | Fahey et al. (29) | 19 | М | 27.5 | Untrained | 18 | 6 | 3.0 | | 15 | Isometric | QF | 180 |
| Laughman et al. (45) 20 M/W 23.5 Untrained 25 5 5.0 10 12.50 Isometric QF 120 Owens and Malone (59) 10 M/W 21 Untrained 10 1.5 6.7 10 Isometric QF 145 Owens and Melone (59) 10 M/W 21 Untrained 5 1.5 3.3 10 Isometric QF 145 McMiken et al. (54) 9 M/W 21.3 10 3 3.3 10 Isometric QF 150 Romero et al. (65) 9 W 21.6 Untrained 10 5 2.0 15 Isometric QF 150 Eriksson et al. (28) 9 20 Trained (student) 25 5 5.0 ca. 24 12 Isometric QF 90 Kots and Chwilon (39) 16 17 Trained (judo) 16 2.5 6.4 10 10 Isometric QF 90 Kots and Chwilon (39) 19 10 M 18 Untrained | | 8 | M/W | 24 | Untrained | 15 | 5 | 3.0 | 10 | | Isometric | QF | 120 |
| Laughman et al. (45) 20 M/W 23.5 Untrained 25 5 5.0 10 12.50 Isometric QF 120 Owens and Malone (59) 10 M/W 21 Untrained 10 1.5 6.7 10 Isometric QF 145 Owens and Melone (59) 10 M/W 21 Untrained 5 1.5 3.3 10 Isometric QF 145 McMiken et al. (54) 9 M/W 21.3 10 3 3.3 10 Isometric QF 150 Romero et al. (65) 9 W 21.6 Untrained 10 5 2.0 15 Isometric QF 150 Eriksson et al. (28) 9 20 Trained (student) 25 5 5.0 ca. 24 12 Isometric QF 90 Kots and Chwilon (39) 16 17 Trained (judo) 16 2.5 6.4 10 10 Isometric QF 90 Kots and Chwilon (39) 19 10 M 18 Untrained | Currier and Mann (24) | 9 | M/W | 24 | Untrained | 15 | 5 | 3.0 | 10 | | Isometric | QF | 120 |
| Owens and Malone (59) 10 M/W 21 Untrained 10 1.5 6.7 10 Isometric QF 145 Owens and Melone (59) 10 M/W 21 Untrained 5 1.5 3.3 10 Isometric QF 145 McMiken et al. (54) 9 M/W 21.3 10 3 3.3 10 Isometric QF 150 Romero et al. (65) 9 W 21.6 Untrained 10 5 2.0 15 Isometric QF 115 Eriksson et al. (28) 9 20 Trained (student) 25 5 5.0 ca. 24 12 Isometric QF 90 Eriksson et al. (28) 4 22 Trained (student) 15 4 3.8 6 6 Isometric QF 90 Kots and Chwilon (39) 16 17 Trained (judo) 16 2.5 6.4 10 10 Isometric TS Kots and Chwilon (39) 19 16 2.5 6.4 10 10 Isometric TS Anzil et al. (2) 10 M 18 Untrained 52 8 6.5 Isometric QF 90 Massey et al. (52) 16 M 22 Trained (marines) 9 40 Isometric UB Diff. | Laughman et al. (45) | 20 | M/W | 23.5 | Untrained | 25 | 5 | 5.0 | 10 | 12.50 | Isometric | QF | 120 |
| Owens and Melone (59) 10 M/W 21 Untrained 5 1.5 3.3 10 Isometric QF 145 McMiken et al. (54) 9 M/W 21.3 10 3 3.3 10 Isometric QF 150 Romero et al. (65) 9 W 21.6 Untrained 10 5 2.0 15 Isometric QF 115 Eriksson et al. (28) 9 20 Trained (student) 25 5 5.0 ca. 24 12 Isometric QF 90 Eriksson et al. (28) 4 22 Trained (student) 15 4 3.8 6 6 Isometric QF 90 Kots and Chwilon (39) 16 17 Trained (judo) 16 2.5 6.4 10 10 Isometric TS Kots and Chwilon (39) 19 16 2.5 6.4 10 10 Isometric TS Anzil et al. (2) 10 M 18 Untrained 52 8 6.5 Isometric QF 90 Massey et al. (52) 16 M 22 Trained (marines) 9 40 Isometric UB Diff. | | 10 | M/W | 21 | Untrained | 10 | 1.5 | 6.7 | | | Isometric | | 145 |
| Romero et al. (65) 9 W 21.6 Untrained 10 5 2.0 15 Isometric QF 115 Eriksson et al. (28) 9 20 Trained (student) 25 5 5.0 ca. 24 12 Isometric QF 90 Eriksson et al. (28) 4 22 Trained (student) 15 4 3.8 6 6 Isometric QF 90 Kots and Chwilon (39) 16 17 Trained (judo) 16 2.5 6.4 10 10 Isometric TS Kots and Chwilon (39) 19 16 2.5 6.4 10 10 Isometric TS Anzil et al. (2) 10 M 18 Untrained 52 8 6.5 Isometric QF 90 Massey et al. (52) 16 M 22 Trained (marines) 9 40 Isometric UB Diff. | | 10 | M/W | 21 | Untrained | 5 | 1.5 | 3.3 | 10 | | Isometric | QF | 145 |
| Romero et al. (65) 9 W 21.6 Untrained 10 5 2.0 15 Isometric QF 115 Eriksson et al. (28) 9 20 Trained (student) 25 5 5.0 ca. 24 12 Isometric QF 90 Eriksson et al. (28) 4 22 Trained (student) 15 4 3.8 6 6 Isometric QF 90 Kots and Chwilon (39) 16 17 Trained (judo) 16 2.5 6.4 10 10 Isometric TS Kots and Chwilon (39) 19 16 2.5 6.4 10 10 Isometric TS Anzil et al. (2) 10 M 18 Untrained 52 8 6.5 Isometric QF 90 Massey et al. (52) 16 M 22 Trained (marines) 9 40 Isometric UB Diff. | McMiken et al. (54) | 9 | M/W | 21.3 | | 10 | 3 | 3.3 | 10 | | Isometric | QF | 150 |
| Eriksson et al. (28) 4 22 Trained (student) 15 4 3.8 6 6 Isometric QF 90 Kots and Chwilon (39) 16 17 Trained (judo) 16 2.5 6.4 10 10 Isometric TS Kots and Chwilon (39) 19 16 2.5 6.4 10 10 Isometric TS Anzil et al. (2) 10 M 18 Untrained 52 8 6.5 Isometric QF 90 Massey et al. (52) 16 M 22 Trained (marines) 9 40 Isometric UB Diff. | Romero et al. (65) | 9 | W | | Untrained | 10 | 5 | 2.0 | | 15 | Isometric | | 115 |
| Kots and Chwilon (39) 16 17 Trained (judo) 16 2.5 6.4 10 10 Isometric TS Kots and Chwilon (39) 19 16 2.5 6.4 10 10 Isometric TS Anzil et al. (2) 10 M 18 Untrained 52 8 6.5 Isometric QF 90 Massey et al. (52) 16 M 22 Trained (marines) 9 40 Isometric UB Diff. | Eriksson et al. (28) | 9 | | 20 | Trained (student) | 25 | 5 | 5.0 | ca. 24 | 12 | Isometric | QF | 90 |
| Kots and Chwilon (39) 16 17 Trained (judo) 16 2.5 6.4 10 10 Isometric TS Kots and Chwilon (39) 19 16 2.5 6.4 10 10 Isometric TS Anzil et al. (2) 10 M 18 Untrained 52 8 6.5 Isometric QF 90 Massey et al. (52) 16 M 22 Trained (marines) 9 40 Isometric UB Diff. | Eriksson et al. (28) | 4 | | 22 | Trained (student) | 15 | 4 | 3.8 | 6 | 6 | Isometric | QF | 90 |
| Kots and Chwilon (39) 19 16 2.5 6.4 10 10 Isometric TS Anzil et al. (2) 10 M 18 Untrained 52 8 6.5 Isometric QF 90 Massey et al. (52) 16 M 22 Trained (marines) 9 40 Isometric UB Diff. | | 16 | | | | | 2.5 | | 10 | 10 | | | |
| Anzil et al. (2) 10 M 18 Untrained 52 8 6.5 Isometric QF 90 Massey et al. (52) 16 M 22 Trained (marines) 9 40 Isometric UB Diff. | , , | | | | 4 / | | | | | | | | |
| Massey et al. (52) 16 M 22 Trained (marines) 9 40 Isometric UB Diff. | | 10 | M | 18 | Untrained | | | 6.5 | | | Isometric | | 90 |
| | | 16 | М | 22 | Trained (marines |) | 9 | | | 40 | Isometric | | Diff. |
| | Mean value (SD) | 10.6 (4.9 |) | 22.8 (2.8 | | 16.3 | 5.0 | 3.5 (1.4 | 1) | 17.5 (10. | 5) | | 108.1 (39.3 |
| (6.9) (2.2) | | | - | | - | (6.9) | | | - | | - | | |

| | JOH | Stimo | ulation parame | eters | | | | | | | Stimula intens | |
|-----------------------------------|----------------------|------------------------------------|-----------------|-------|-----|------|-------|--------|------|-----------|-------------------|----|
| Authors | Type of current | Type of stimulator | Impulse form | μѕ | Hz | mA | on(s) | off(s) | Duty | Rise/fall | %MVC | ø |
| Avila et al. (5) | Russian current | Physiotonus Slim, Bioset, Brazi | Sinus | 200 | 50 | 44 | | | | | | |
| Avila et al. (5) | Russian current | Physiotonus Slim, Bioset, Brazi | Sinus | 200 | 50 | 58 | | | | | | |
| Speicher et al. (69) | Biphasic | Miha Bodytec | Rectangular | 350 | 85 | | 60 | 60 | 50.0 | | | |
| Paillard I (60) | Biphasic | CEFARTM MYO 4, Sweden | Rectangular | | 80 | 60.8 | 6 | 18 | 25.0 | 1.8/1.2 | | |
| Paillard (60) | Biphasic | CEFARTM MYO 4, Sweden | Rectangular | | | 67.6 | 10 | 6 | 62.5 | 1.8/1.2 | | |
| Babault et al. (6) | Biphasic | Compex Medical SA | Rectangular | | | 50 | 5 | 15 | 25.0 | | 60 | 60 |
| Holcomb (33) | Russian current | Forte 400 Combo E-Stimulator | | | 90 | | 15 | 45 | 25.0 | | 20.4 | 20 |
| Matsuse et al. (53) | Biphasic | | Rectangular | | 20 | 10 | 2 | | | | 25-30 | 27 |
| Jubeau et al. (38) | Biphasic | Compex Medical SA | Rectangular | 400 | .75 | 70.5 | 6.25 | 20 | 23.8 | 1.5/0.75 | 82 ± 19 | 82 |
| Gondin et al. (31) | Biphasic - | Compex Medical SA | Rectangular | | 75 | 72.5 | 6.25 | 20 | 23.8 | | 68 + 14 | 68 |
| Maffiuletti et al. (49) | Biphasic | Compex Medical SA | Rectangular | | 75 | 64 | 6.25 | 20 | 23.8 | 1.5/0.75 | 61-79 | 70 |
| Boeckh-Behrens and Mainka (13) | Biphasic | Body Transformer | Rectangular | | 80 | | 4 | 4 | 50.0 | 0/0 | | |
| Boeckh-Behrens and Mainka (13) | Biphasic | Body Transformer | Rectangular | 350 | 80 | | 4 | 4 | 50.0 | 0/0 | | |
| Kreuzer et al. (41) | Biphasic | Body Transformer | Rectangular | 350 | 85 | | 4 | 4 | 50.0 | | | |
| Gondin et al. (31) | Biphasic | Compex Medical SA | Rectangular | | 75 | 75 | 4 | 20 | 16.7 | 1.5/0.75 | 68 ± 13 | 68 |
| Brocherie et al. (19) | Biphasic | Compex 2 Medical SA | Rectangular | | 85 | | 4 | 20 | 16.7 | | 60 | 60 |
| Boeckh-Behrens and Bengel (12) | Biphasic | Body Transformer | Rectangular | 350 | 80 | | 4 | 4 | 50.0 | 0/0 | | |
| Boeckh-Behrens and Bengel (12) | Biphasic | Body Transformer | Rectangular | 350 | 80 | | 4 | 10 | 28.6 | 0/0 | | |
| Herrero et al. (32) | Biphasic | Compex Medical SA | Rectangular | 400 | 120 | 40 | 3 | 30 | 9.1 | 0.75/0.5 | | |
| Herrero et al. (32) | Biphasic | Compex Sport Medical SA | Rectangular | | 120 | 66 | 3 | 30 | 9.1 | 0.75/0.5 | | |
| Parker et al. (61) | | Forte 200 electrical stimulator | | 200 | 50 | 82.8 | 10 | 50 | 16.7 | | 63 | 63 |
| Parker et al. (61) | | Forte 200 electrical stimulator | | 200 | 50 | 75.3 | 10 | 50 | 16.7 | | 69.5 | 69 |
| Malatesta et al. (50) | Biphasic | Compex 2 Medical SA | Rectangular | 400 | 120 | 80 | 4.25 | 31.5 | 11.9 | 0.7/0.5 | | |
| Boeckh-Behrens et al. (14) | Biphasic | Body Transformer | Triangular | 350 | 80 | | 8 | 4 | 66.7 | 0.3/0 | | |
| Dervisevic et al. (26) | | BIMED 999S | | | | | | | | | 10 | 10 |
| Bircan et al. (10) | Interference current | Myomed 932 | Sinus | | 80 | 44 | 13 | 50 | 20.6 | 2/1s | | |
| Bircan et al. (10) | Interference current | | Sinus | | 80 | 43.5 | 13 | 50 | 20.6 | 2/1s | | |
| Bircan et al. (10) | Biphasic symmetr. | Myomed 932 | | 100 | | 44 | 13 | 50 | 20.6 | | | |

TABLE 8. Overview EMS parameters 2/3.

| | 900 | | Stimulation para | meters | S | | | | | | Stimulat intensi | |
|----------------------------------|---------------------|--------------------------|------------------|--------|-------|------|--------|---------|------|-----------|---------------------|------|
| Authors | Type of current | Type of stimulator | Impulse form | μѕ | Hz | mA | on (s) | off (s) | Duty | Rise/fall | %MVC | ø |
| Maffiuletti et al. (47) | Biphasic | Compex Sport Medical SA | Rectangular | 400 | 120 | 90 | 3 | 17 | 15.0 | 0.75/0.5 | 60 | 60 |
| Maffiuletti et al. (47) | Biphasic | Compex Sport Medical SA | Rectangular | 400 | 120 | 90 | 3 | 17 | 15.0 | 0.75/0.5 | 60 | 60 |
| Maffiuletti et al. (48) | Biphasic | Compex Sport Medical SA | Rectangular | 400 | 75 | 60 | 4 | 20 | 16.7 | | 50-70 | 60 |
| Boeckhh-Behrens and Treu (15) | Biphasic | Body Transformer | Triangular | 350 | 80 | | 8 | 4 | 66.7 | 0.3/0 | | |
| Maffiuletti et al. (46) | Biphasic | Compex 2 Medical SA | Rectangular | 400 | 100 | 80 | 3 | 17 | 15.0 | | 80 | 80 |
| Colson et al. (22) | Biphasic | Compex 2 Medical SA | Rectangular | 240 | 80 | 100 | 3 | | | | 60-70 | 65 |
| Hortobágyi et al. (35) | Alternating current | Electrostim 180-2 | Sinus | | 50 | 52.5 | | | 50.0 | | 49-106 | 77.5 |
| Willougby and Simpson (76) | C | Dynatron 500 | Sinus | 100 | 50 | | 25 | 180 | 12.2 | | | |
| Willougby and Simpson (76) | | Dynatron 500 | Sinus | 100 | 50 | | 25 | 180 | 12.2 | | | |
| Hortobágyi et al. (34) | Biphasic | Electrostim 180-2 | Sinus | | 50 | 52 | | | 50.0 | | 70-150 | 110 |
| Willoughby and | Z-ip-riddio | Dynatron 500 | Symmetric | 100 | 50 | | 30 | 120 | 20.0 | | 85 | 85 |
| Simpson (75) | | | | | 1 | | | | | | | |
| Willoughby and Simpson (75) | 3 51 | Dynatron 500 | | 100 | 50 | | 30 | 120 | 20.0 | | 85 | 85 |
| Pichon et al. (62) | Biphasic | Stiwell Stimulator | Rectangular | 300 | / 80 | | 6 | 20 | 23.1 | | 60 | 60 |
| Mmethodin et al. | Alternating current | Compex Sport Medical SA | 9 | 200 | 70 | | 5 | 15 | 25.0 | | 63.2 ± 8.6 | 63.2 |
| Miller and | Monophasic | Prototype Uni. Compiegne | Rectangular | 200 | 90 | 59.9 | 5 | 25 | 16.7 | 1-2/ | 30.6 | 30.6 |
| Thepaut-Mathieu (55) | | | J | | | | | | | | | |
| Balogun et al. (8) | Monophasic | HVGS | 2-Peak (needle) | 70 | 20 | | 10 | 50 | 16.7 | | | |
| Balogun et al. (8) | Monophasic | HVGS | 2-Peak (needle) | 70 | 45 | | 10 | 50 | 16.7 | | | |
| Balogun et al. (8) | Monophasic | HVGS | 2-Peak (needle) | 70 | 80 | | 10 | 50 | 16.7 | | | |
| Rich (64) | Russian current | Electrostim 180-2 | Sinus | 100 | 50 | 18.4 | 10 | 50 | 16.7 | 5/0 | 62.3 | 62.3 |
| Rich (64) | Russian current | Electrostim 180-2 | Sinus | 100 | 50 | 34 | 10 | 50 | 16.7 | 5/0 | 45.5 | 45.5 |
| Rich (64) | Russian current | Electrostim 180-2 | Sinus | 100 | 50 | 42.8 | 10 | 50 | 16.7 | 5/0 | 37.2 | 37.2 |
| Rich (64) | Russian current | Electrostim 180-2 | Sinus | 100 | 50 | 54.7 | 10 | 50 | 16.7 | 5/0 | 29.6 | 29.6 |
| Portmann and Montpetit (63) | Monophasic comp | BMR Powerstim | Rectangular | 400 | 100 | | 10 | 50 | 16.7 | | 82.2-93.6 | 87.9 |
| Portmann and Montpetit (63) | Monophasic comp | BMR Powerstim | Rectangular | 400 | 100 | | 10 | 50 | 16.7 | | 81.1-94.8 | 87.9 |
| Venable et al. (73) | Biphasic | Intelect VMS Stimulator | Rectangular | 200 | 50 | | 15 | 60 | 20.0 | 5/0 | 33-110 | 71.5 |
| Delitto et al. (25) | F | VersaStim 380 Miami | Triangular | | 75 | 200 | 11 | 180 | 5.8 | | 112 | 112 |
| Soo et al. (68) | Russian current | Electrostim 180-2 | Sinus | | 50 | 40 | 15 | | 2.0 | 5/0 | 50 | 50 |
| Soo et al. (68) | Russian current | Electrostim 180-2 | Sinus | | 50 | 40 | 15 | | | 5/0 | 50 | 50 |
| Lai et al. (43) | Biphasic asymetr. | Minidyne 3 UK | Asymmetric | 200 | 50 | _ | 5 | 5 | 50.0 | | 56.6-72.7 | 64.6 |
| Lai et al. (43) | Biphasic asymetr. | Minidyne 3 UK | Asymmetric | 200 | 50 | | 5 | 5 | 50.0 | | 43.4-60.5 | 52 |
| Cabric and Appell (21) | Alternating current | ., = | Rectangular | 150 | 2,500 | 40 | 10 | 50 | 16.7 | | | |
| Cabric and Appell (20) | Alternating current | | Rectangular | 200 | 50 | 40 | 5 | 35 | 12.5 | | | |

| Authors | | Stimulation | parameters | | |
|-----------------------------------|---------------------|--------------------------------|-----------------|---------------|------------|
| Addiois | Type of current | Type of stimulator | Impulse form | μs | Hz |
| Cabric and Appell (20) | Alternating current | | Rectangular | 200 | 2000 |
| Kubiak et al. (42) | Russian current | Electrostim 180-2 | Sinus | | 50 |
| Alon et al. (1) | Biphasic symmetr. | Intelect VMS stimulator Proto | Symmetric | 200 | 50 |
| Alon et al. (1)† | Biphasic symmetr. | Intelect VMS stimulator Proto | Symmetric | 200 | 50 |
| St. Pierre et al. (70) | Alternating current | Dr. Kots personal apparatus | Sinus | | 50 |
| St. Pierre et al. (70) | Alternating current | Dr. Kots personal apparatus | Sinus | | 50 |
| weekslf et al. | Monophasic | EMPI, Inc., Fridley, MN | Rectangular | | 75 |
| Nobbs and Rhodes (57) | Faraday Strom | Model F283, Multitone Electric | Rectangular | | 60 |
| Nobbs and Rhodes (57) isokinetic. | - Faraday Strom | Model F283, Multitone Electric | Rectangular | | 60 |
| Selkowitz (67) | Russian current | Electrostim 180-2 | Sinus | 450 | 50 |
| Boutelle et al. (17) | Russian current | Electrostim 180 | Sinus | | 50 |
| Stefanovska and Vodovnik (71) | Monophasic | | Sinus | 300 | 25 |
| Stefanovska and Vodovnik (71) | Monophasic | | Rectangular | 300 | 25 |
| Mohr et al. (56) | Monophasic | Intellect Model 500 HVG | 2-Peak (needle) | 45 | 50 |
| Fahey et al. (29) | Biphasic asymetr. | Medtronic 3108 | Rectangular | | 50 |
| Fahey et al. (29) | Biphasic asymetr. | Medtronic 3107 | Rectangular | | 50 |
| Currier and Mann (24) | Russian current | Electrostim 180-2 | Sinus | 100 | 50 |
| Currier and Mann (24) | Russian current | Electrostim 180-2 | Sinus | 100 | 50 |
| Laughman et al. (45) | Russian current | Electrostim 180 | Sinus | | 50 |
| Owens and Melone (59) | Russian current | Electrostim 180 | Sinus | 200 | 50 |
| Owens and Melone (59) | Russian current | Electrostim 180 | Sinus | 200 | 50 |
| McMiken et al. (54) | Faraday Strom | Faradic Unit Model GF01 | | 100 | 75 |
| Romero et al. (65) | Faraday Strom | SP5 Faradic | | | 2,000 |
| Eriksson et al. (28) | | Grass. Quincy. Mass | Rectangular | 500 | 200 |
| Eriksson et al. (28) | | Grass, Quincy, Mass | Rectangular | 500 | 200 |
| Kots and Chwilon (39) | Russian current | Dr. Kots personal apparatus | Rectangular | | 50 |
| Kots and Chwilon (39) | Russian current | Dr. Kots personal apparatus | Rectangular | | 50 |
| Anzil et al. (2)* | | Modotto personal stimulator | • | | |
| Massey et al. (52) | | Isotron stimulator | Rectangular | | 1,000 |
| Mean value (SD) | | | • | 261.6 (131.9) | 151.4 (399 |

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Review of Influence of Training Regimen and Stimulation Parameters on Effectiveness

| Authors | | W | Stimulation parameter | ers | | Stimulation intensity | |
|------------------------------------|-------------|-----------|-----------------------|-------------|-----------|-----------------------|------------|
| Additions | mA — | on (s) | off (s) | Duty | Rise/fall | %MVC | Ø |
| Cabric and Appell (20) | 40 | 5 | 35 | 12.5 | | | |
| Kubiak et al. (42) | | 15 | 50 | 23.1 | 5/0 | 75 | 75 |
| Alon et al. (1) | 122 | 12.5 | 7.5 | 62.5 | | | |
| Alon et al. (1)† | 122 | 12.5 | 7.5 | 62.5 | | | |
| St. Pierre et al. (70) | 39.5 | 10 | 50 | 16.7 | | 80-100 | 90 |
| St. Pierre et al. (70) | 39.5 | 10 | 50 | 16.7 | | 80–100 | 90 |
| weekslf et al. | 62 | | | | | 20-40 | 30 |
| Nobbs and Rhodes (57) | 15.00 | 10 | 50 | 16.7 | | | |
| Nobbs and Rhodes (57) isokinetic.† | 15.00 | 3 | 50 | 5.7 | | | |
| Selkowitz (67) | 59 | 10 | 120 | 7.7 | 0.6-3/ | 91 | 91 |
| Boutelle et al. (17) | | | | | | | |
| Stefanovska and Vodovnik (71) | 73.1 | 10 | 50 | 16.7 | | 5 | 5 |
| Stefanovska and Vodovnik (71) | 43.12 | 10 | 50 | 1/6.7 | | 5 | 5 |
| Mohr et al. (56) | | 10 | 10 | 50.0 | 3.3/0 | | |
| Fahey et al. (29) | 45 | 10 | 5 | 66.7 | 2/0 | | |
| Fahey et al. (29) | 45 | 10 | 5 | 66.7 | 2/0 | | |
| Currier and Mann (24)† | 45.8 | 15 | 50 | 23.1 | 5/0 | 66.7 | 66.7 |
| Currier and Mann (24) | 55.3 | 15 | 50 | 23.1 | 5/0 | 88.4 | 88.4 |
| Laughman et al. (45) | 62.5 | 15 | 50 | 23.1 | 5/0 | 33 | 33 |
| Owens and Melone (59) | 46.5 | 15 | 50 | 23.1 | 3.5/ | 60 | 60 |
| Owens and Melone (59) | 34.6 | 15 | 50 | 23.1 | 3.5/ | 39 | 39 |
| McMiken et al. (54) | | 10 | 50 | 16.7 | | 80 | 80 |
| Romero et al. (65) | | 4 | 4 | 50.0 | | | |
| Eriksson et al. (28) | | 15 | 15 | 50.0 | | | |
| Eriksson et al. (28) | | 6 | 6 | 50.0 | | | |
| Kots and Chwilon (39) | | 10 | 50 | 16.7 | | >50 | 50 |
| Kots and Chwilon (39) | | 10 | 50 | 16.7 | | >50 | 50 |
| Anzil et al. (2)* | | 10 | 300 | 3.2 | | | |
| Massey et al. (52) | | 10 | | | | | |
| Mean value (SD) | 58.6 (30.5) | 10.1 (7.9 | 9) 40.8 (38.2) | 27.0 (17.5) | | | 60.8 (24.8 |

17% of the studies investigated the upper body. Beyond that, only 8% analyzed the effects of whole-body stimulation on the muscle (12–15,41,66,69) (cf. Tables 4–6).

Besides these basic data, the analysis performed during this study showed that several parameters are used to influence stimulation effectiveness (i.e., the training outcome).

Impulse Type

Analysis of the selected studies revealed a large deviance in the types of EMS stimulators used. A stimulator produced by the company "Compex" was used in 37% of the trials conducted after 1994. Before then, an "Electrostim 180" device was used (28%). In the recent years, new stimulators, such as the "Bodytransformer" or the EMS stimulator manufactured by "Miha Bodytec" have been in use for whole-body EMS.

The impulse type that these EMS stimulators produced in the selected studies was biphasic in 40% of the cases and monophasic in 12%. In 21% of the trials, a so-called "Russian current" was used. This type of impulse was delivered by the "Electrostim 180." An alternating sinus current was applied in only 8% of the studies. Furthermore, only 5% of the trials were accomplished with an Interference or Faraday current. The rest of the studies (15%) provided no information about the impulse type used.

It is noteworthy that, from 1994 onward, most of the trials (67%) used biphasic impulses (cf. Tables 5–9).

Impulse Form

Forty percent of the impulses were delivered with a square or rectangular form, and another 27% used an alternating sinus impulse form. In 15% of the studies, stimulation was performed with symmetrical, asymmetrical, triangular, and peak impulses. The rest of the trials (10%) did not comment on the impulse form.

Impulse Width

On average, an impulse width of 261 ± 132 microseconds was used. A width between 200 and 400 microseconds was applied in 48% of the study designs. In 27% of the studies, no information about impulse width was provided.

Impulse Frequency

The regulated frequency varied between 25 and 2,500 Hz. Frequencies over 1,000 Hz were not included in the mean value (cf. (21,52,65)).

Impulse Intensity

To regulate the maximum impulse intensity, this value was either defined as the maximal tolerated amperage or as the maximal comfortable amperage (mA). This value varied between 10 and 200 mA.

Impulse on Time

In the sample of trials, the time over which a single impulse stimulated a muscle group varied between 3 and 60 seconds. The interval between 2 impulses varied between 4 seconds and 3 minutes.

Stimulation Intensity

Intensity was defined and regulated on the basis of the MVC during the retest of a particular muscle and expressed as a percentage. The values ranged between 5 and 112% of the MVC (cf. Tables 5–9). In 42% of the studies, no information was provided on the intensity in relation to the MVC.

COMPARISON OF CERTAIN TRAINING REGIMENS AND THEIR TRAINING EFFECTIVENESS

Studies reviewed in this section applied a stimulation intensity of 63.2 \pm 19.8% MVC and documented significant strength gains (p < 0.05) in maximal strength, speed strength, jumping and sprinting ability, and power.

Duration of Training Period

As far as the training period is concerned, the authors achieved significant gains in maximal strength within 3–6 weeks $(3.2 \pm 0.9 \text{ sessions per week})$ of duration regardless of the local EMS method and the subject's level of fitness (e.g., gains in isometric Fmax after isometric EMS: trained athletes $4.3 \pm 1.9 \text{ weeks}$ (20-22,28,55,63,67); elite athletes $3.5 \pm 0.7 (46,62)$). Moreover, it was possible to reveal that an extension of the training period beyond 6 weeks without varying the stimulus shows no further significant strength gains (p < 0.05). Only one study was able to achieve an increase in isometric Fmax with <3 weeks of stimulation (21).

The analysis of the effects on jumping ability revealed that a stimulation period of as many as 4 weeks is adequate for enhancing jumping strength (trained subjects, elite athletes 4.4 ± 1.5 weeks (6,39,46,60)). For example, Brocherie et al. (19) documented a decrease in jumping values (SJ -8.4; CMJ -6.1; DJ -4.8) within 3 weeks of study duration (3 sessions per week) although they used stimulation parameters similar to the ones employed in other successful trials (cf. 6.39,46,50,60,75,76).

In summary, regardless of the EMS method used, the analysis revealed that a stimulation period in a range of 4–6 weeks (3.2 ± 0.9 sessions per-week) shows positive effects for enhancing strength parameters, jumping and sprinting ability, and power.

Number of Stimulation Sessions per Week

Regarding strength gains achieved with local EMS methods (isometric EMS, dynamic EMS), the analysis showed that 3 sessions per week (over 4–6 weeks) can be adequate to achieve significant gains in isometric Fmax >30% in trained subjects (isometric EMS 4.8 \pm 2 sessions per week (20–22, 28,55,63,67); dynamic EMS 3 \pm 0 sessions per week (57,63)) and elite athletes (isometric EMS 3.5 \pm 0.7 sessions per week (46,62); combination EMS 3 \pm 0 sessions per week plus 3 \pm 0 sessions per week of additional plyometric jump training (47)).

The studies by Parker et al. (61) and Soo et al. (68) indicated that less than 3 sessions per week (2 ± 0) might not suffice to activate strength adaptations. However, the analysis of the results could not show a correlation between the number of

stimulation sessions per week and the strength gains in isometric Fmax. The same results were found and transferred in all EMS methods.

In the view of dynamic Fmax, the analysis documented strength gains of >30% with local EMS methods in trained subjects and elite athletes (isometric EMS 3.8 ± 2.2 sessions per week (6,25,39,75); dynamic EMS 3 ± 0 sessions per week (75,76)).

The use of 3 sessions per weeks could also be seen in studies focussing the Mmax. The analysis documented significant gains in concentric and eccentric Mmax of trained subjects training 3.3 ± 0.5 sessions per week with isometric EMS (22,26,28,63) and 2.5 ± 0.6 sessions per week with dynamic EMS (5,57) and elite athletes training 2.8 ± 0.5 sessions per week in isometric EMS (6,19,46,62) and 3.5 ± 0.7 sessions per week in dynamic EMS (75,77).

Regarding the whole-body EMS methods, the analysis showed that all trials using whole-body EMS only used 2 stimulation sessions per week (2 ± 0 sessions per week (12–15,41,66,69). These studies only achieved minor increases in maximal strength (isometric Fmax <10%; dynamic Fmax <10%) and in jumping ability (not significant). However, studies showed that power (Pmax) and parameters of speed strength (RFD; force impulse) can be significantly developed with 2 sessions per week over a 4-week stimulation period (cf. (66,74)).

In summary, the present investigation reveals that applying an EMS stimulus above training threshold ≥3 times a week (over 4.4 ± 1.5 weeks) shows positive effects for enhancing strength parameters. To ensure regeneration and to not overstress the subjects muscular system, we recommend not to exceed 3 sessions per week for enhancing the strength parameters at hand.

Duration of a Stimulation Session

On the basis of results from meaningful studies, the analysis revealed that an average stimulation duration of 17.52 ± 10.56 minutes in each of 3 sessions per week (3.2 ± 0.9 sessions per week, 4–6 weeks) with a sufficient intensity can be adequate to activate strength adaptations with EMS methods (isometric EMS 16.5 ± 10 minutes; combination EMS 25.3 ± 12.4 ; whole-body EMS 14.0 ± 7.4).

Regarding strength gains in maximal strength, the analysis showed that elite athletes increased the isometric Fmax >20% with isometric EMS by using a stimulation duration of 14.0 \pm 2.8 minutes per session (46,62) and trained subjects with 11 \pm 1.4 minutes per session (28,63). For significantly increasing dyn Fmax Portmann and Montpetit (63) applied dynamic EMS of 10 minutes per session (3 sessions per week). Increase in dyn Fmax in trained and elite athletes with isometric EMS was achieved with a stimulation duration of 15.5 \pm 9.7 minutes per session (3.8 \pm 2.2 sessions per week) (6,25,39,75).

Regarding gains in vertical jump in trained and elite athletes the analysis showed that significant increases were achieved with a stimulation duration of 13.3 ± 2.8 minutes (4 ± 2 sessions per week) in isometric EMS (6,39,46,60) and with 24.0 ± 11.1 minutes per session with combination EMS (32,47,73). Similar results were shown in sprint ability of elite athletes using isometric EMS $(12.0 \pm 0 \text{ minutes per session } (19,62))$.

In comparison, the results of trials using whole-body EMS methods showed that a duration of 15 minutes can be assumed to be sufficient for stimulation to activate strength adaptations and thus increasing strength abilities (e.g., dyn Fmax 11.8 \pm 5.7 (12,13,15)). No significantly higher increases were found because of a longer stimulation duration per session (cf. (14,69)). The investigation further revealed a significant correlation ($p \leq 0.05$) between stimulation duration for whole-body isometric EMS (5–15 minutes) and the increase of dynamic Fmax within a duty cycle of <50% (50–28.6%), which supports the previous thesis. Furthermore, the whole-body EMS methods can simultaneously stimulate several muscle groups at the same time (15 minutes), whereas local methods only stimulated one muscle group.

In summary, a stimulation duration in the range of 10–15 minutes appears to be sufficient for enhancing the current strength parameters with all of the analyzed EMS methods.

COMPARISON OF CERTAIN ELECTROMYOSTIMULATION PARAMETERS AND CORRELATION TO TRAINING EFFECTIVENESS

All studies reviewed in the following section documented significant strength gains (p < 0.05) by applying EMS over a stimulation period of 4.4 ± 1.5 weeks with 3.2 ± 0.9 session per week.

Stimulation Intensity

The analysis in this study revealed that training intensity is the primary parameter for training effectiveness. It was possible to show that the level of stimulation intensity (MVC) of the trained muscle determines the training effectiveness. According to this, the analysis demonstrated a significant correlation (r=0.724, p<0.05) between %MVC (65.2 \pm 7.6% MVC) and the strength gain in isometric Fmax (29.1 \pm 8.0%) for trained subjects after isometric EMS (cf. (20–22,28,32,52,55,63,67)). A significant correlation (r=0.433, p<0.05) with the same parameters could be seen in untrained subjects as well (63.6 \pm 16.4% MVC (2,8,17,24,31,32,38,42,43,45,47,49,51,53,54,56,59,61,68,71)).

Regarding significant strength gains in isometric Fmax with local isometric EMS, meaningful studies applied a stimulation intensity of 68.6 ± 27.9% MVC in trained subjects (20–22,28,55,63,67) and 70 ± 14.1% MVC in elite athletes (46,62). Similar results were shown in dynamic EMS (trained subjects 87.9% MVC (63)); and isometric combination EMS (elite athletes 60.0% MVC (47)). In regard to increases in vertical jump height with isometric EMS meaningful studies achieved significant gains with ≥50% MVC in trained subjects (39,60) and with 57.0 ± 4.1% MVC in elite athletes (6,46). Similar MVC values were documented in studies using

combination EMS for enhancing jump ability (65.8 \pm 8.1% MVC (47,73)).

In studies investigating whole-body EMS methods no information about the level of MVC was given (12–15,41,66,69).

According to the results, in all of the analyzed categories, significant positive changes can be related to an MVC level of ≥50%. Holcomb (33) and Stefanoska and Vodovnik (71) confirm these results. The stimulation intensity (MVC) they used (20.4%; 5% MVC) was too low to produce a stimulus above the training threshold to cause strength adaptations. Furthermore, in the study by Rich et al. (64) significant strength increases in isometric Finax were only achieved in the group for which a stimulation intensity of >50% MVC was applied.

In summary, it can be assumed that a stimulation intensity of ≥50% MVC is required to produce a stimulus in the muscles that has a sufficient intensity to activate strength adaptations. The analysis further showed that the MVC level is mainly influenced by the impulse intensity (mA), the stimulation frequency (Hz) and the impulse width (microseconds). For the sum of these stimulation parameters, there is a recommendable range or level, which will be given below.

Impulse Intensity

Regarding the effect of isometric EMS on isometric Fmax, the analysis showed a significant relationship (p < 0.05) between impulse intensity (mA) and the muscle contraction (MVC) in untrained subjects (1,2,8,17,24,31,38,42,43,45,51,53,54,64,68). The results reveal the influence of impulse intensity (mA) on stimulation intensity (%MVC).

Regarding significant strength gains in isometric Fmax with local EMS methods, meaningful studies applied an impulse intensity of ≥40 mA (trained subjects 56.5 ± 23.4 mA (20–22,55,67); elite athletes 80 mA (46)). Similar results were shown in studies focusing isokinetic Mmax in trained subjects and elite athletes. (e.g., isometric EMS 65.0 ± 21.2 mA (6,46); dynamic EMS 53.7 ± 6.8 mA (5,34,35,77)) and jumping ability (e.g., isometric EMS 63.5 ± 15.2 mA (6,46,60)).

In studies investigating whole-body EMS methods no information about the level of impulse intensity (mA) was given (12–15,41,66,69).

Nonetheless, the analysis showed that high MVC levels (and consequently significant strength gains) were predominately achieved with an impulse intensity of ≥50 mA. However, it is difficult to quantify this, because the impulse intensity (mA) is influenced by several individual factors such as tissue structures and pain perception.

In summary, the analysis revealed that an impulse intensity of ≥50 mA positively influences the generation of a stimulation intensity of ≥50% MVC.

Impulse Frequency

The present analysis showed evidence that an impulse frequency of ≥50 Hz is a precondition for developing a high stimulation intensity (%MVC) and thus for producing a training stimulus that activates strength adaptations. The studies at hand showed significant gains in strength

parameters and jumping and sprinting ability by a use of 68.6 ± 31.7 Hz on average.

Studies focusing the increase of isometric Fmax with local EMS methods used stimulation frequencies of \geq 50 Hz in trained subjects (isometric EMS 80 \pm 21.6 Hz (21,22,55,63); dynamic EMS 80 \pm 28.3 Hz (57,63)).

Similar frequencies were shown in studies that significantly increased dynamic Fmax of elite athletes (isometric EMS 68.0 ± 23.9 Hz (6,25,39,75); dynamic EMS 62.5 ± 17.7 Hz (76,77)).

Also, in studies focusing on isokinetic Mmax a stimulation frequency of \geq 50 Hz could be seen in trained subjects (isometric EMS 68.7 \pm 11.5 Hz (22,26,63); dynamic EMS 60.0 \pm 20.0 Hz (5,34,35,57,63)) and elite athletes (isometric EMS 91.3 \pm 10.3 Hz (6,19,46,62); dynamic EMS 62.5 \pm 17.7 Hz (75,77)).

Regarding performance, independent of the subjects' level of fitness, significant gains in jumping ability were achieved by the use of 82.5 ± 23.6 Hz in isometric EMS (6,39,46,60) and by 95.8 ± 39.7 Hz in combination EMS (32,47,73). Furthermore, it was possible to increase the sprint strength with a stimulation frequency of 82.5 ± 2.5 Hz in isometric EMS (elite athletes (19,64)) and 120.0 Hz in combination EMS (untrained (33)).

In comparison to local EMS methods, studies using whole-body EMS methods applied a stimulation frequency of ≥ 80 Hz (82.5 \pm 3.5 Hz (12–15,41,66,69) and achieved significant gains in maximal strength of \leq 10% (isom Fmax/dyn Fmax), speed strength (RFD; force impulse) and power of trained subjects.

In summary, according to the results of this study, we can suggest that independent of the EMS method a stimulation frequency of ≥60 Hz can be sufficient for developing a high stimulation intensity (MVC) to enhance maximal strength, speed strength, power, and jumping and sprinting ability.

Impulse Width

Regarding the level of impulse width (microseconds), several authors recommend the use of a medium-width (cf. (16)). Accordingly, in this review overall, 48% of the trials used impulse widths of 200–400 microseconds (261.64 \pm 131.88 microseconds, e.g., (14,32,37,38,46,49)).

The analysis showed that impulse width influences the intensity of muscle contraction (%MVC) when combined with the abovementioned stimulation parameters in the recommended range. However, it was not possible to show any direct correlation between impulse width and %MVC. For example, the studies performed by Willoughby and Simpson (75) and by Portmann and Montpetit (63) achieved intensities of >85% MVC with an impulse width of 100 microseconds and 400 microseconds.

Compared to the impulse widths used in isometric EMS (isom Fmax 292.5 \pm 135.3 microseconds (20–22,27,55,63,67); dyn Fmax 350.0 \pm 70.7 microseconds (46,62); isok Mmax 345.0 \pm 127.9 microseconds (22,26,28,63); vertical jump 416.7 \pm

28.9 microseconds (6,46,60); sprint time 275.0 ± 25.0 microseconds (19,62)) narrower impulses were generally noticeable in studies using dynamic EMS (dyn Fmax 200.0 ± 173.2 microseconds (63,75,76); isok Mmax 200.0 ± 122.5 microseconds (5,63,75,76); vertical jump 100 microseconds (76)). Depending on the type of combination EMS method (isometric, dynamic) similar impulse widths were used (e.g., isometric Fmax 333.3 ± 115.5 microseconds; isometric combination EMS (32,47,73)).

Similar to local EMS methods whole-body EMS studies also applied a medium-width impulse of 350.0 ± 0 microseconds (12–15,41,66,69)) and achieved significant gains in maximal strength of ≤10% (isom Fmax/dyn Fmax), speed strength (RFD; force impulse) and power in trained subjects.

On the basis of the results of the present analysis we assume that impulse widths in a range of 200–400 microseconds are sufficient for producing a stimulus above training threshold and thus activate strength adaptations.

Stimulation Ratio (Duty Cycle)

The stimulation ratio (duty cycle) is defined as ratio of on-time to the total cycle time (% duty cycle = 100/[total time/on-time]).

Regarding the stimulation ratio (duty cycle) in local EMS methods, the analysis showed that a duty cycle between 20 and 25% shows positive effect on strength enhancements. It was possible to reveal a significant correlation ($\phi < 0.5$) between a duty cycle of 26.5 \pm 13.7% within isometric EMS and strength gains in isometric Fmax for untrained subjects (23.5 \pm 8.9% duty cycle (1,2,8,15,24,31,38,42,43,45,51,53,54,64,68)).

In regard to the enhancement in isom Fmax (32.3 \pm 16.6%) with isometric EMS, similar duty cycles were documented in trained subjects (19.0 \pm 14.1% duty cycle (20,21,28,55,63,67)) and elite athletes (19.1 \pm 5.7% duty cycle (46,62)). Similar duty cycles were also found in studies that significantly increased isokinetic Mmax (19.9 \pm 4.8% duty cycle (6,19,46,62)), jumping (20.4 \pm 5.3% duty cycle (6,39,46,60)), and sprinting ability (19.9 \pm 3.1% duty cycle (19,62)) with isometric EMS. In addition, in studies using dynamic EMS a duty cycle in the same range was favored (e.g., dyn Fmax 16.1 \pm 5.5% duty cycle (75,76); jumping ability 12.1% duty cycle (76)).

The combination EMS methods revealed that significant gains up to +62% in isometric Fmax are possible with a duty cycle of $14.7 \pm 5.5\%$ (32,47,73) when supplemented by traditional strength training (2.7 \pm 0.6 sessions per week (40,57,86)).

In the case of the whole-body EMS method, a stimulation design with a duty cycle between 28.6 and 66.7% was used (12–15,41,69). Whole-body EMS methods documented significant gains in maximal strength, speed strength (RFD; force impulse), and power. No gains in vertical jump ability could be documented.

Regarding the on-time (contraction time), the analysis showed that impulse on-times of 3-10 seconds in particular positively influence strength adaptations in trained subjects and elite athletes when using isometric EMS method (e.g., isom Fmax 7.8 \pm 3.7 seconds (7,31,42,43,51); dyn Fmax 6.3 \pm 3.5 seconds (22,26,28,63); vertical jump 6.0 \pm 2.9 seconds (6,39,46,60); sprint 5.0 \pm 1.0 seconds (19,62)). Concerning dynamic EMS methods Willoughby and Simpson (75,76) achieved significant gains >20% in dyn Fmax and vertical jump by using longer impulse on-times \geq 20 seconds (27.5 \pm 3.5 seconds).

Studies using whole-body EMS applied an on-time of 4.6 ± 1 seconds per contraction (41,69) to enhance isom Fmax (<10%). For increasing dyn Fmax (<15%) studies applied an on-time of 4.9 ± 1.7 seconds per contraction (12,13,15). Whole-body combination methods showed significant gains in dyn Fmax <10% by a use of an on-time of 7.5 ± 0.9 seconds (14,69).

In contrast, for significantly developing speed strength (RFD; force impulse) and power (including 2max) Speicher et al. (69) applied an on-time of 60 ± 0 seconds per contraction (50% duty cycle). However, theses results have to be stated with caution because only few international studies are published in this section.

In summary, on the basis of the results independent of the local EMS method short impulse on-times (contraction time) in a range of 3–10 seconds combined with a duty cycle of 20–25% showed positive effects for enhancing maximal strength, speed strength, and jumping and sprinting ability. Whole-body EMS methods revealed that an on-time of 60 seconds with a 50% duty cycle can be effective for developing parameters of speed strength (RFD/force impulse) and power.

For regeneration time (impulse interval), the analysis showed evidence that a stimulation ratio of 20–25% duty cycle is adequate for recovery between the contractions and thus positively influences strength adaptation.

DISCUSSION

On the basis of the results, we conclude that a stimulation intensity of ≥50% MVC is required to produce a stimulus in the muscles that has sufficient intensity to activate strength adaptations. Further, the analysis revealed that the %MVC level is mainly influenced by the impulse intensity (mA), the stimulation frequency (Hz), and the impulse width (microseconds). According to this, we conclude that independent of the EMS method, an impulse intensity of ≥50 mA in connection with a stimulation frequency of 76.4 ± 20.9 Hz and an impulse width of 306.9 ± 105.1 microseconds positively influence the generation of a stimulation intensity of ≥50% MVC and thus generate a stimulus above a training threshold that activates strength adaptations. In regard to the training regimen when applying this combination of stimulation parameters, we conclude that a stimulation period in a range of 4-6 weeks with 3 sessions per week (10-15 minutes per session) and a stimulation ratio in a range of 3-10 seconds on-time (20-25% duty cycle) are sufficient for enhancing maximal strength, speed strength, jumping and sprinting ability, and power in trained and elite athletes.

Regarding training regimens, the analysis revealed that in trained subjects and elite athletes, 3 sessions per week over a stimulation period of 4–6 weeks are adequate for activating strength adaptations. In regard to maximal strength, some studies showed significant gains even after a 3-week period (cf. (20,43,54)). In contrast, speed strength, and jumping and sprinting ability show a higher complexity in movement and are therefore influenced by several parameters such as coordination and neural activation. In regard to the results, these parameters can show delays in adaptation. In keeping with this, the analysis showed that a stimulation period of ≥4 weeks (3 sessions per week) is sufficient to also ensure enhancements in speed strength and jumping and sprinting ability.

When applying an EMS stimulus according to the parameters described above independent of the EMS method used a higher number of training session (>3 sessions per week) within a stimulation period of 4–6 weeks can overstress the subject's muscular system and thus hampering strength adaptations.

According to that studies investigating the effects of EMS on creatinkinase activity showed that the electrical stimulus can cause significantly more stress in the muscular system and therefore exhibits higher creatinkinase activity compared to voluntary muscle contraction exercise (cf. (12,13,37,41)). Consequently, EMS requires a higher interval between the training sessions to not overstress the muscular system and ensure strength adaptations.

For example, Boeckh-Behrens (12) showed that, compared to traditional strength training, the stress on the muscular system is about 40% higher after intensive EMS. Boeckh-Behrens came to the conclusion that the level of stimulation intensity is responsible for the level of creatinkinase activity, whereas stimulation duration has no influence (cf. (13)).

Regarding the development of creatinkinase activity, Boeckh-Behrens documented results showing that the subjects still exhibited high values after long periods ranging from 24 hours to 4 days. Further stimulation within this time of decomposition would result in a summation of creatinkinase activity (72), which in turn can overstress the athletes' muscular system. Consequently, the size of the interval between 2 EMS sessions is very important for activating strength adaptations. According to Kreuzer et al. (41), the muscular system acclimatizes to the electrical stimulus in as little as 3 weeks, which in turn results in reduced creatinkinase activity. For example, introducing the electrical stimulus to the subjects before starting with the actual stimulation period (acclimatization period) might prevent extreme summation of creatinkinase activity and muscle soreness.

Regarding the creatinkinase activity related to the individual level of fitness, the studies analyzed in this review could not show a difference between untrained subjects and trained athletes. Steinacker et al. (72) assume that elite athletes show less creatinkinase activity compared to untrained subjects after EMS, because they have more experience in performance training and therefore a greater tolerance to highly intensive training. This would indicate that elite athletes can be stimulated with higher intensity and or with a higher number of training sessions per week.

As mentioned above, the stimulation intensity influences the level of creatinkinase activity. Accordingly, we suggest that the stimulation intensity is an important parameter for planning strength training. In contrast to voluntary exercise, with EMS, the intensity is defined by the level (%) of MVC. As shown in this review, significant enhancements in maximal strength, speed strength, and motor abilities such as jumping and sprinting have been demonstrated in connection with stimulation intensities of ≥50% MVC in combination with the training regimens described above.

Regarding the stimulation intensity, the analysis showed that intensities of ≥50% MVC were mostly produced with biphasic impulses (e.g., (6,31,37,49)). Monophasic current flows from one electrode to the other in a fixed direction that can create an ionic current within the tissue. This can result in unpleasant side effects such as electrolysis and risk of chemical burning. On the contrary, biphasic currents flow between both electrodes and thus have a zero net current (44). Accordingly, biphasic currents are perceived as more pleasant for the subjects' muscles (3,16). For this reason, subjects are able to tolerate biphasic currents better, which means that the impulses can be more intensive. Consequently, biphasic currents offer advantages for applying high stimulation intensities and therefore have a positive influence on the enhancement of strength abilities

Regarding the stimulation parameters, the present analysis revealed that the frequency, intensity, and width of the impulses used are the most relevant stimulation parameters that influence stimulation intensity. Therefore, these parameters must be taken into consideration to generate a stimulus that activates strength adaptations.

In regard to the influence of the impulse intensity (mA) on stimulation intensity (MVC) Lake (44) was able to show in his study that the muscle contraction force can be regulated by varying the level of amperage (mA). Accordingly, a higher impulse intensity (mA) results in a higher %MVC. However, the impulse intensity depends on the resistance of different tissue structures. According to Bossert et al. (16), a major portion of the resistance is because of the resistance of the skin. Therefore, it is not possible to precisely determine the impulse intensity (mA) that ultimately reaches the muscle. Most studies used the maximum pain threshold (maximum tolerated amperage) to regulate the maximum impulse intensity (e.g. (19,31,38,41,46)). Nonetheless, the pain threshold depends on the subject's individual pain perception and on the particular muscle. Studies showed that the subjects quickly experience pain acclimatization through EMS. Accordingly, to maintain a certain level of stimulation intensity the impulse intensity (mA) has to be continuously enhanced to adapt to the changing situation (cf., e.g., (46,50)). However, Cabric and Appell (21) mentioned that when increasing the

impulse intensity a maximal level of muscle contraction force is achieved with intensities over 100 mA, and no further positive effects might appear. Furthermore, maximal impulse intensities and thus a high level of muscle tension will limit dynamic movements. Therefore, in dynamic EMS methods, the impulse intensity (mA) has to be regulated to ensure unlimited movement.

Depending on the muscle structure, the amperage (mA) required to penetrate the skin (44) can vary. Consequently, trained subjects with a lower percentage of fat revealed a lower pain threshold compared to untrained subjects. This is because muscular systems with less fat offer lower resistance, which results in a higher intensity within the muscle. Furthermore, because the amperage (mA) is defined by the load that flows though a cross section of a lead per time unit (16), impulse intensity also depends on the specific area of application. Consequently, the size of the EMS electrodes influences impulse intensity within the muscle.

The analysis showed that high MVC levels (and consequently significant strength gains) were predominately achieved with an impulse intensity of ≥50 mA. However, research revealed that the impulse intensity is highly influenced by the individuals' pain perception, by the condition of the muscular system and by motivation (cf. (16)). In connection with the findings described above we conclude that the value of amperage is difficult to quantify, and therefore, it is rather a guide value than a decisive factor for training control.

In regard to the stimulation frequency, research in EMS showed that different stimulation frequencies activate different types of muscle fiber (4). For example, in a fiber spectrum of 2-15 Hz, mostly slow-twitch fibers (type 1) will be stimulated. According to Appell (4), Fast-twitch fibers (type 2), which are responsible for the development of high forces, may not contract below 35 Hz. A further increase in frequency then leads to a complete tetanus of the stimulated muscle. Appell (4) acts on the assumption that this maximal muscle activation can be enhanced up to a frequency of 70 Hz. According to Blümel (11), however, a complete tetanus will be reached between a frequency of 50 and 200 Hz, whereas Bossert et al. (16) came to a different conclusion; they assert that maximum stimulation for type-2 fibers takes place at around 50-60 Hz. There are different opinions about the level of stimulation frequency in the current state of research. Although Kramer (40) achieved the highest Mmax with 20 Hz, Cometti (23) recommends impulse frequencies from 50 to 100 Hz. Binder-Macleod and Guerin (9) came to a similar result. They see higher frequencies between 60 and 100 Hz as more effective.

In regard to the results of this review in connection with the findings described above, we conclude that impulse frequencies in a range between 50 and 100 Hz are sufficient for generating high stimulation intensities (MVC) when applied in combination with an adequate impulse intensity and impulse width.

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The minimal impulse width is defined by the minimal time required (chronaxie) for the swell intensity to create an action potential within the stimulated motor neuron. According to Bossert et al. (16), this impulse width lies in the range of 80–800 microseconds. Longer impulse durations (wider impulses) result in proportionately deeper and more intensive muscle stimulation (cf. (7,16)) and thus more motor units will be recruited. However, the presence of algesic substances increases as the width rises.

Hultmann et al. (36) have held that a minimum impulse width of 500 microseconds is needed to develop high forces. Their results show that lowering the impulse width significantly reduces the MVC produced. Bossert et al. (16) came to the conclusion that no widths above 500 microseconds should be used, because impulses above this level would be unpleasant or even painful. They assume that no sensitive reactions are to be expected on a level around 300 microseconds. For this reason, they recommend a level between 300 and 400 microseconds.

In connection with the results of this review, we conclude as a compromise that an impulse width in a range between 200 and 400 microseconds is sufficient for generating high stimulation intensities ≥50% MVC. Furthermore, the application will also activate the deeper motor units without being unpleasant for the athlete, but the stimulus will be intensive enough to cause strength adaptations.

Regarding the stimulation ratio, the analysis revealed a predominant use of short impulse on-times of 6.0 ± 2.4 seconds in all EMS methods for enhancing strength abilities.

In voluntary exercise the stimulation ratio is used to specify the training program in relation to certain strength abilities. According to Weineck (74), in traditional strength training, speed strength, and maximal strength will be trained using impulse on-times (contraction time) between 3 and 6 seconds per contractions, whereas muscle hypertrophy will be activated after 10 seconds of duration. In particular, maximal strength and speed strength are both influenced by coordination and neuronal activation. The analysis revealed that with EMS the strength abilities are mainly increased by neuronal adaptations and less through hypertrophy. For example, the increase in power went in hand with an increase in vmax, which again is influenced by several neuronal factors such as coordination and neuronal activation (69). Accordingly, in regard to the results of this review, we can state that short impulse on-times also positively influence the enhancement in maximal strength and speed strength with EMS.

Regarding the interval between 2 single impulses, Appell (3) sees the off-phase as regeneration time for recovering energy depots and for restitution of the motor end plate. He assumes that a ratio between 1:1 and 1:5 is optimal. According to Edel (27), intervals that are too short cause the muscles to fatigue rapidly, which reduce the effect of training.

In summary, we conclude that the use of short impulse on-times (contraction time) between 3 and 10 seconds positively influence the enhancement of maximal strength and speed strength and thus jumping and sprinting ability and power. For regeneration time (impulse interval) we assume that a stimulation ratio with a 20–25% duty cycle and a short duration of 3–10 seconds ensures sufficient recovery and thus enables strength adaptations.

Regarding the enhancements gained for the analyzed strength parameters that were shown in the first study (cf. (30)) in relation to training regimen and stimulation parameters, this study demonstrated that untrained subjects are able to significantly enhance all strength parameters within 3–6 weeks with a wide variety in training patterns, whereas elite athletes only have small improvement

As mentioned before, EMS is an intensive training method that can require a higher interval between sessions than voluntary exercise. Accordingly, EMS has to be applied with caution. Especially untrained subjects have to be trained with caution because of their lower resistance to intensive load. Overloading the subjects' muscular system by for example applying EMS with a high stimulation intensity in combination with not enough regeneration time between the sessions can inhibit or delay strength adaptations. Consequently, significant strength gains were often first demonstrated in retesting after a rehabilitation (detrain) period of 2-6 weeks (cf. (32,41,46,49,69)). Employing a load that was too low, on the other hand, resulted in a rapid decrease (within 2-4 weeks) in achieved strength gains after posttesting (cf. (32,43,53)), or led to a lack of any significant enhancements in posttesting (17,24,33,41,52,55,58,61,65,68,69,71).

In contrary, several trials revealed that, when EMS was applied with optimal load, the achieved strength gains can be kept at a constant level in untrained and trained subjects for up to 4 weeks after posttesting without doing any exercise (cf. (7,17,32,38,41,43,60,69)). In the case of elite athletes, the analysis showed that continuing the usual highperformance training after posttesting can keep or even enhance the achieved strength gains for up to 6 weeks (46,47,50). In keeping with this, for example, Maffiuletti et al. (56,57) showed further strength increases in the vertical jump height of elite basketball players (+3% SJ, +17% CMJ) and elite volleyball players (+1.6% SJ, +5% CMJ, ±0% DJ) within 6 weeks after posttesting. On the basis of these results, we can assume that athletic training or strength training after finishing the stimulation period is able to maintain the achieved levels of strength and jumping

Regarding changes in strength gains after posttest the analyzed data suggest a relationship between stimulation intensity and the period over which it is possible to maintain the achieved gains. Furthermore, the changes in strength after posttesting (detraining) showed that gains achieved over longer periods (4 weeks) are more likely to remain constant after posttesting (7). As seen in traditional training, also in

EMS training gains achieved in a short period of time (<4 weeks) decreased more quickly after posttesting (43).

PRACTICAL APPLICATIONS

The following guidelines for strength training control were developed because of the results of this review series and include recommendations for developing maximal strength and speed strength and jumping and sprinting ability, and power in strength training especially in high-performance sports.

The present analysis revealed that a stimulation intensity of ≥50% MVC in connection with the training regimen in the recommended range (4-6 weeks, 3 sessions per week) is a precondition for activating strength adaptations. To generate a stimulus above training threshold, coaches should apply an impulse width in a range of 200–400 microseconds and an impulse frequency of 50–100 Hz. For regulating the impulse intensity and thus generating an adequate level of stimulation intensity (%MVC), trained and elite athletes should approach a submaximal to maximum level of mA (≥50 mA).

Before applying EMS with this intensity (≥50% MVC), EMS training intensity should be increased step by step. This helps to accommodate individual reactions to the EMS stimulus, athletes will be introduced to it before starting the actual stimulation period, and coaches can set the training level of impulse intensity (mA) according to the individual's maximum tolerated level more easily without risking overstressing the subjects' muscular system. When this is done, the subjects are able to get used to the electrical stimulus that is significantly more intensive compared to voluntary contraction stimulus in traditional weight training which can cause significantly higher damage in the athletes' muscular system. Furthermore, this will reduce muscle soreness in the beginning.

When setting the stimulation intensity for training, compared to trained subjects and elite athletes, untrained subjects should not focus on the maximum tolerated impulse intensity (mA) in order not to overstress the muscular system. For acclimatization, we recommend to start with 1 session per week. Within the actual stimulation period, untrained subjects should train a maximum of 2 times a week with a submaximal intensity. Trained subjects and elite athletes should start with 2 sessions per week with submaximal intensity before applying EMS with individual maximum intensity within the actual training period. In general, regardless of their level of fitness, subjects should not exceed 3 sessions per week (including additional voluntary strength training).

The stimulation intensity (%MVC) is influenced by the level of impulse intensity (mA) and depends on individual perception and structure of the muscle. To maintain the level of MVC during the training period and thus ensure strength adaptations, the impulse intensity (mA) has to be carefully and constantly enhanced to account for acclimatization. The impulse frequency, impulse width, impulse type, and stimulation ratio should stay on the defined level during training period (4–6 weeks).

To maintain the achieved strength gains, athletes should integrate a specific strength training (maximal strength, speed strength) or athletic training (sprinting, jumping, coordination) into their daily training (minimum 1 sessions per week) after finishing the simulation period. If continuing with EMS training, a variation of stimulation parameters alters the training stimulus and can thus show positive effects on maintaining or even further enhance the achieved strength gains.

Although the first study revealed the effectiveness of EMS, EMS should be used as an additional training alternative in strength training and not as a complete replacement. Regardless of the EMS method used, additional athletic performance training has a positive influence for transferring the strength gains to specific types of movements, such as sprinting or jumping.

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